

Abstract. Capillary viscometry can be a practical technique to provide viscosity estimates for small volumes of fluids. The viscosity can be estimated if the pressure drop, the flow rate and the length of the capillary are known. Non-Newtonian models can be incorporated. By considering the propagation of the flow in the capillary and accepting a power-law approximation for blood viscosity, the consistency index and exponent can be estimated. The aim of this work, was to estimate the viscosity of various blood samples, for flows in a converging, rectangular microfluidic channel. The calculated viscosity was compared with the viscosity measurements produced using a commercial instrument.

Methodology.

Capillary microchannel:

- Convergent geometry.
- Channel width: entrance 5mm, exit 1mm. Depth: ~100 μm, length: 20mm.
- Meniscus velocity: Tracking velocimetry. Local velocity field: μPIV techniques.

Meniscus velocity vs flow length:

- Power-law viscosity model, and Young-Laplace pressure drop^{1,2}.

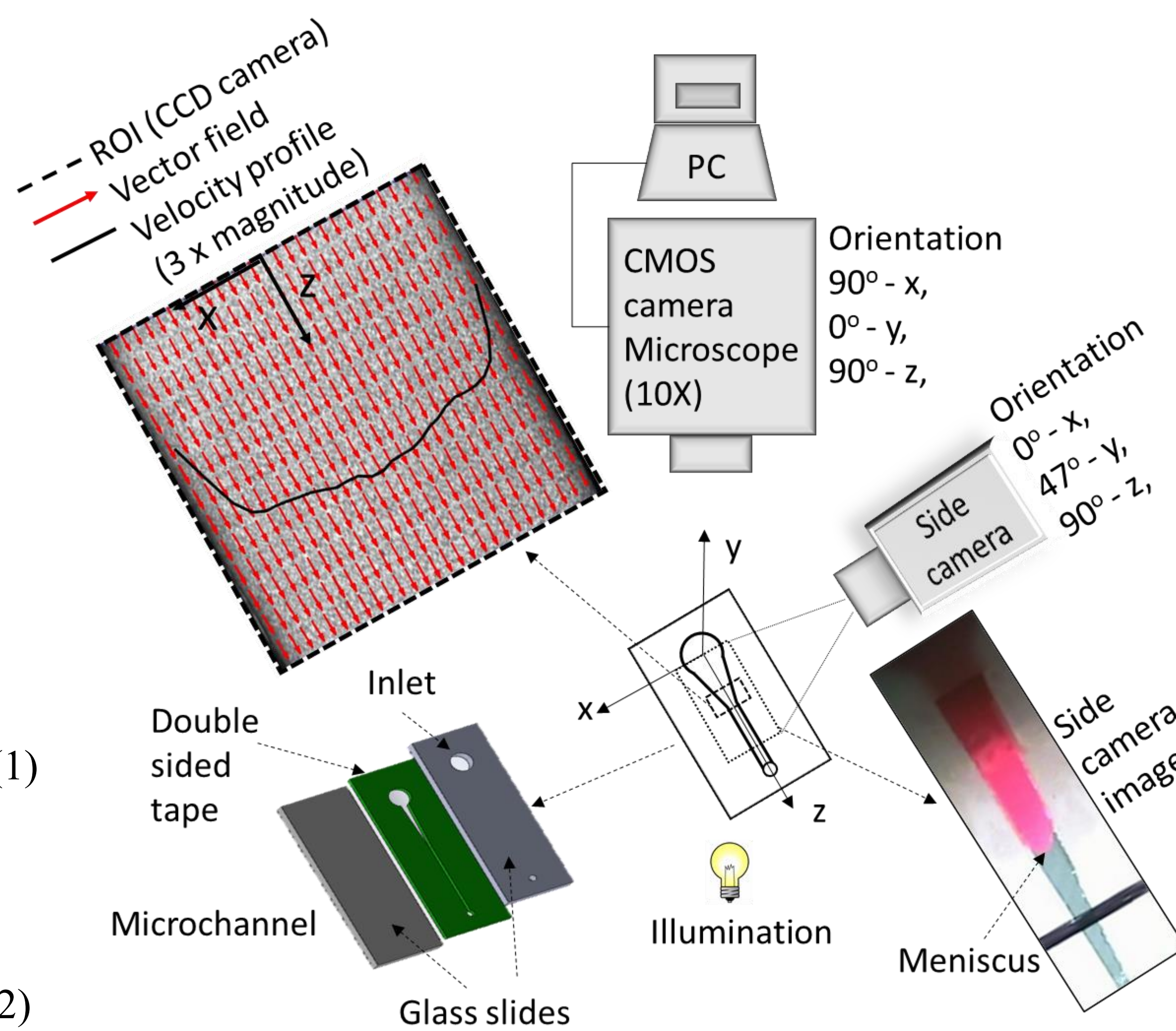
$$V(t)^n = \left(\frac{n}{n+1}\right)^n \left[\frac{\sigma \cos(\theta_c)}{hkL(t)}\right] \left[h^{\frac{n+1}{n}} \left(1 - \frac{n}{2n+1}\right)\right]^n \quad (1)$$

Rearranging (1):

$$\frac{1}{L(t)} = \left(\frac{2n+1}{n}\right)^n \left[\frac{hk}{\sigma \cos \theta} \frac{1}{h^{n+1}}\right] V(t)^n = CV(t)^n \quad (2)$$

$$\log\left(\frac{1}{L(t)}\right) = \log C + n \log V(t) \quad (3)$$

n and k: power law indices,
σ and θ_c: surface tension and contact angle,
h and L: gap and flow length.



Setup^{3,4}:

- CMOS camera: IDT X3, 2000 images, 1250 fps.
- Side camera: JVC TK-C1380 color, 60mm Panasonic lens.
- Microscope: BX51 OLYMPUS, 10X-objective, NA=0.25.
- Image spatial resolution: 1.65 μm/pixel, μPIV analysis: Matlab.

Viscosity measurements:

- Cone-plate, Brookfield LVDT II instrument.
- Viscosity derived at shear rates between 251.2 (starting) and 1.4 s⁻¹ (final).
- Rate sweep mode: 30 seconds measurement time, per shear rate point (17 points).



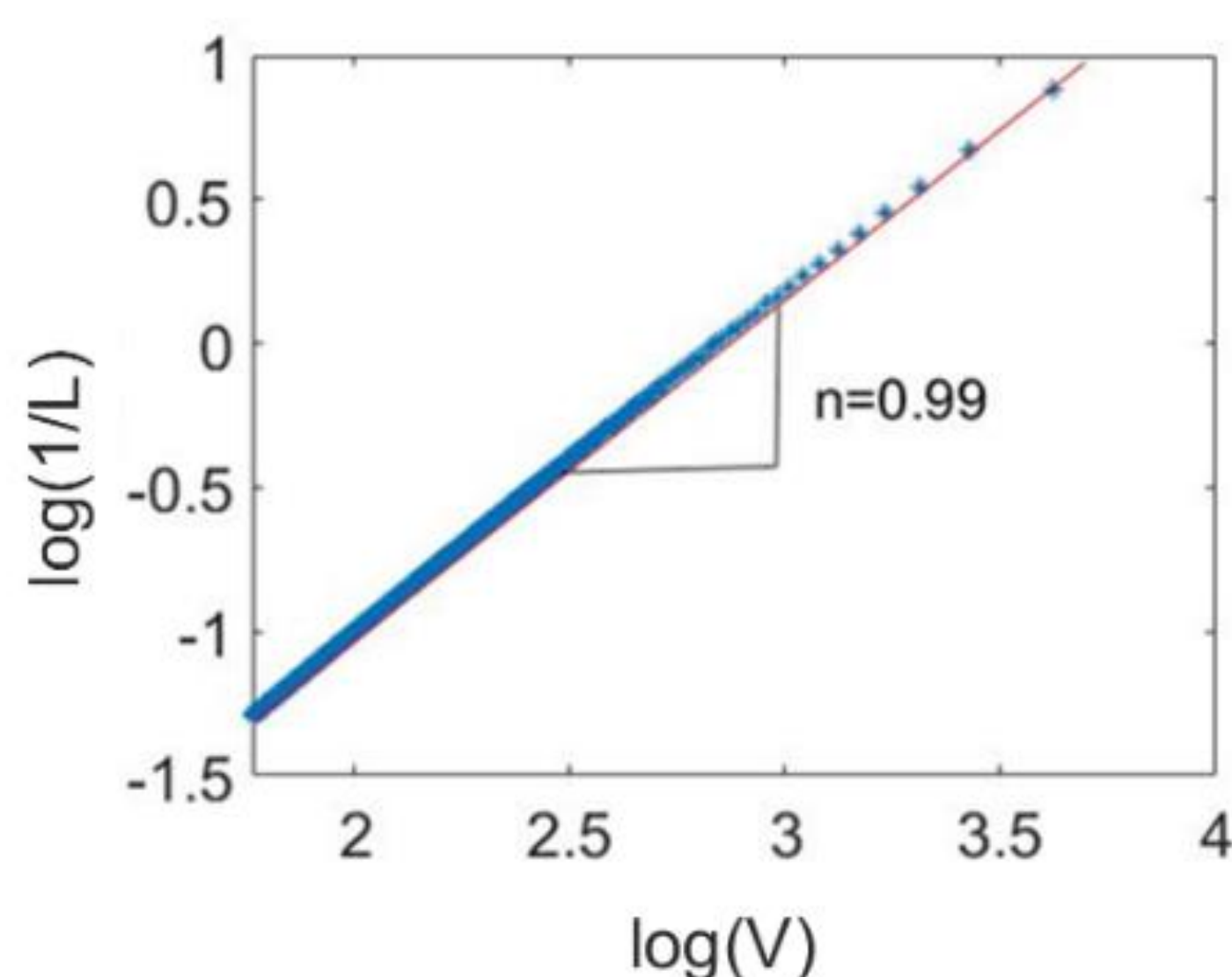
Blood samples:

- 30ml (EDTA anticoagulated) from normal, healthy participants (n=9).
 - Whole blood (WB).
 - RBC suspensions in phosphate buffer saline (PBS).
- (Bioethics ref.: EEBK/EP/2016/18)

Results

Velocity vs flow length.

- Non-aggregative blood suspension.
- RBC aggregation and shear thinning behavior suppressed.
- n~1, Newtonian behaviour.



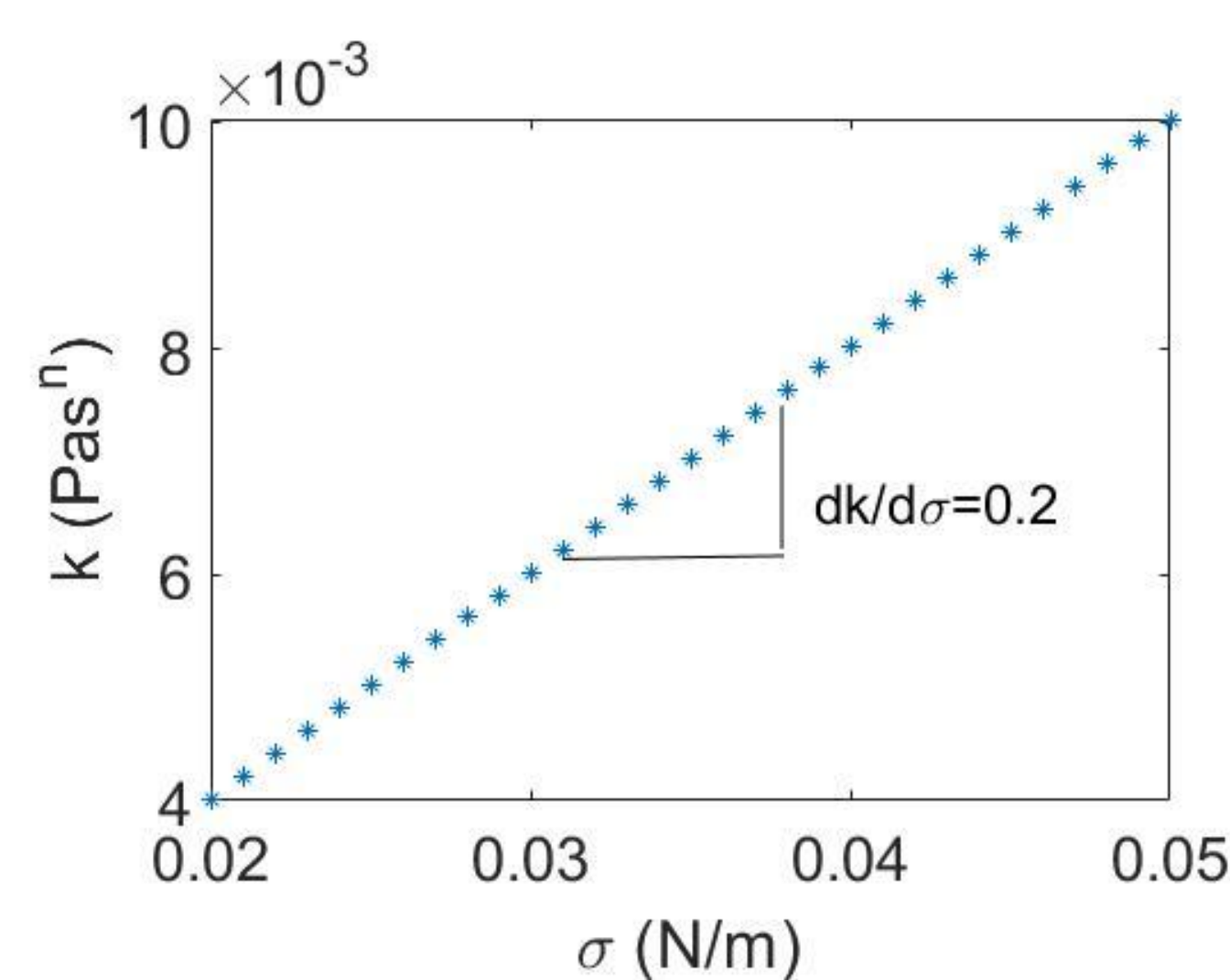
Predicted vs measured viscosity.

- Percent viscosity differences: capillary derivation vs viscometer.
- Aggregative whole blood: strong disaggregation conditions in the flow.
- Shear thinning behavior suppressed.

Shear rate (s ⁻¹)	Sample viscosity difference μ _d (%)	
	Whole Blood	Blood suspension
251.2	-8.94	3.5
125.9	-19.97	-11.33
31.58	-46.75	-39.91
7.875	-67.43	-60.44
3.975	-77.6	-74.99

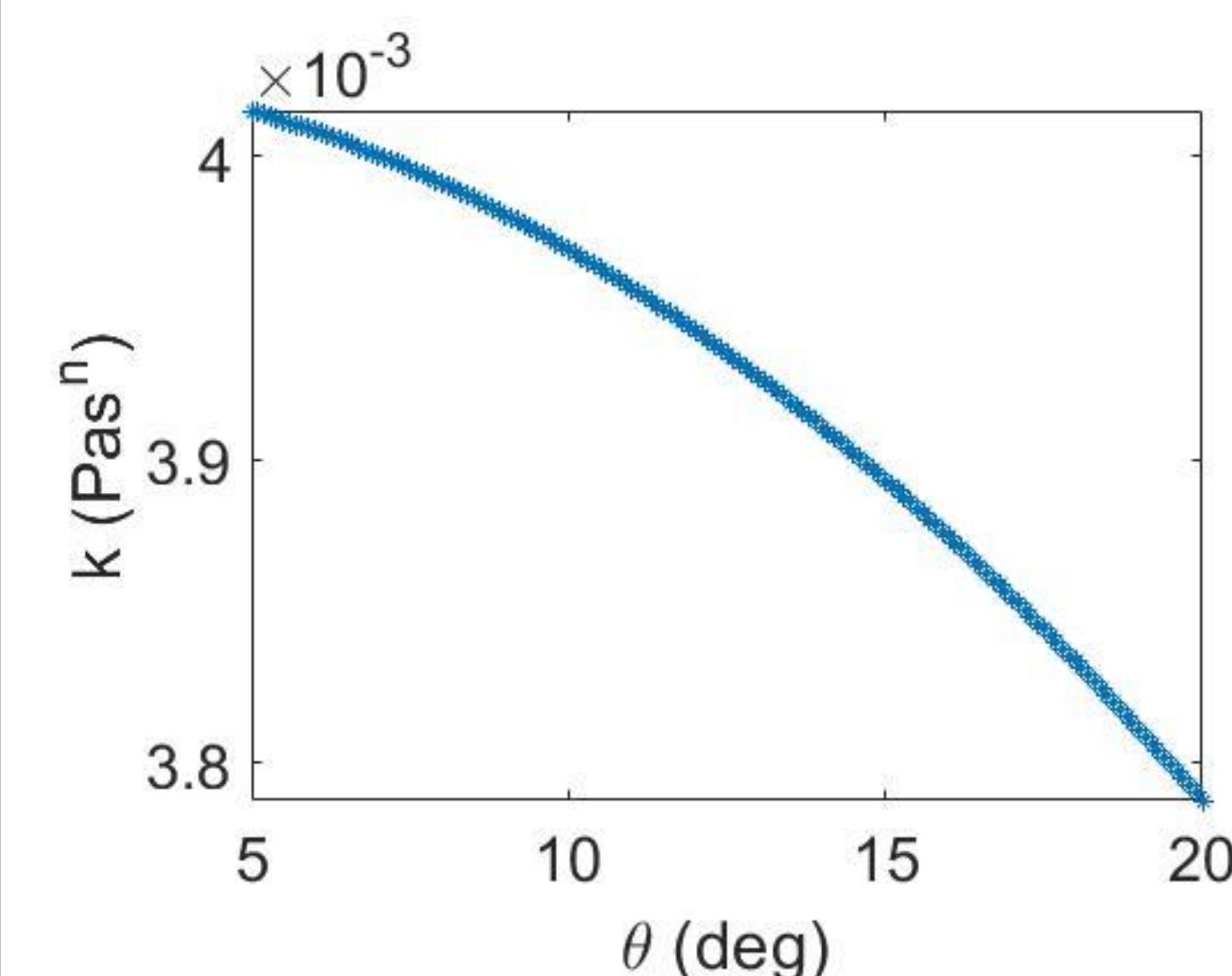
Dependency of k on surface tension.

- k increases 2.5 times for the range of σ: 0.02N/m < σ < 0.05N/m.
- Surface tension affects k.



Dependency of k on contact angle

- k decreased ~ 5%, from θ = 5° to θ = 20°.
- θ does not significantly affect k.



Remarks

- Strong shearing conditions in the flow, and small channel length and duration, suppresses RBC aggregation and shear thinning.
- Calculated viscosity values closer to the high-shear measured viscosity.
- Fluids follow a Newtonian behavior due to reduced RBC aggregation under the specific shearing conditions.
- High shear viscosity of blood can provide information about the general viscous status of the fluid.

Acknowledgments

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